

1 **Comprehensive evaluation and new recommendations in the**  
2 **use of Gafchromic EBT3 film**

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23 **Keywords:** EBT3, radiochromic film, temporal dependence, film dosimetry  
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35 **Abstract**

36 **Background:** Gafchromic film's unique properties of tissue-equivalence, dose-rate independence, and high  
37 spatial resolution make it an attractive choice for many dosimetric applications. However, complicated  
38 calibration processes and film handling limits its routine use.

39 **Purpose:** We evaluated the performance of Gafchromic EBT3 film after irradiation under a variety of  
40 measurement conditions to identify aspects of film handling and analysis for simplified but robust film  
41 dosimetry.

42 **Methods:** The short- (from 5 minutes to 100 hours) and long-term (months) film response was evaluated  
43 for clinically relevant doses of up to 50 Gy for accuracy in dose determination and relative dose  
44 distributions. The dependence of film response on film-read delay, film batch, scanner type, and beam  
45 energy were determined.

46 **Results:** Scanning the film within a 4-h window and using a standard 24-h calibration curve introduced a  
47 maximum error of 2% over a dose range of 1–40 Gy, with lower doses showing higher uncertainty in dose  
48 determination. Relative dose measurements demonstrated <1 mm difference in electron beam parameters  
49 such as depth of 50% of the maximum dose value ( $R_{50}$ ), independent of when the film was scanned after  
50 irradiation or the type of calibration curve used (batch-specific or time-specific calibration curve) if the  
51 same default scanner was used. Analysis of films exposed over a 5-year period showed that using the red  
52 channel led to the lowest variation in the measured net optical density values for different film batches,  
53 with doses >10 Gy having the lowest coefficient of variation (<1.7%). Using scanners of similar design  
54 produced netOD values within 3% after exposure to doses of 1–40 Gy.

55 **Conclusions:** This is the first comprehensive evaluation of the temporal and batch dependence of  
56 Gafchromic EBT3 film evaluated on consolidated data over 8 years. The relative dosimetric measurements  
57 were insensitive to the type of calibration applied (batch- or time-specific) and in-depth time-dependent  
58 dosimetric signal behaviors can be established for film scanned outside of the recommended 16-24 hour  
59 post-irradiation window. We generated guidelines based on our findings to simplify film handling and  
60 analysis and provide tabulated dose- and time-dependent correction factors to achieve this without reducing  
61 the accuracy of dose determination.

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63 **Keywords:** EBT3, radiochromic film, temporal dependence, film dosimetry

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## 65 1 INTRODUCTION

66 Radiochromic film is commonly used for dosimetry in radiation therapy owing to its excellent spatial  
67 resolution, large dynamic dose range, tissue equivalence, dose-rate independence, and energy  
68 independence.<sup>1</sup> Radiochromic film can be used to measure dose and relative dose distributions, including  
69 percent depth dose (PDD) curves, dose homogeneity, and 2D isodose distributions; it is exceptionally  
70 valuable for conformal treatments that involve high dose gradients as well as small field dosimetry.<sup>1,2</sup>  
71 Moreover, film does not require physical or chemical processing and can be robustly handled in ambient  
72 lighting and room temperature conditions<sup>1</sup>. Radiochromic film works as a radiation dosimeter in that  
73 irradiation prompts a polymerization reaction that causes a color change in the irradiated region of the film.  
74 The initial color change is instantaneous upon exposure to ionizing radiation. However, the color's intensity  
75 grows and plateaus after irradiation. Color changes in film are measured quantitatively in terms of optical  
76 density (OD) by using a commercially available flatbed color scanner and analysis software to measure the  
77 amount of light transmitted through irradiated and nonirradiated film.

78 However, radiochromic film is a passive dosimeter, limited by the need for a complicated and time-  
79 consuming calibration and delayed time to readout (recommended 16-24 hours) to allow the polymerization  
80 reaction to stabilize upon irradiation<sup>1,3</sup>. The extent of color changes produced in film also does not correlate  
81 linearly with dose, except when PRESAGE sheets are used.<sup>4,5</sup> Rather, film requires a time-dependent  
82 calibration to convert the measured OD reading to a dose value, because the polymerization reaction never  
83 fully stabilizes<sup>6</sup>. For this reason, it is important to ensure the delay (irradiation to scanning) to be the same  
84 as used for film-calibration, which further limits film usability. Rapidly emerging new technologies, such  
85 as FLASH radiotherapy, are heavily reliant on film dosimetry for beam calibration and experimental  
86 verification of dose due to radiochromic film's established dose-rate independence of up to  $10^{12}$  Gy/s<sup>7-11</sup>.  
87 For radiotherapy with ultra-high dose-rates or "FLASH", traditional dosimeters (except for radiochromic  
88 film) are not usable due to saturation effects. For such ultra-high dose-rates and dose-per-pulse conditions,  
89 as well as extremely short irradiation times, real-time dose monitoring is nontrivial. The read-out delay in  
90 film may be unacceptably long for experiments that rely on quick calculations or rapid adjustment of beam  
91 parameters for which other commercially available dosimeters that can measure radiation in real-time  
92 cannot be used due to large saturation effects.<sup>12</sup>

93 To address the limitations of film dosimetry, we undertook a comprehensive evaluation of how the  
94 signal in Gafchromic EBT3 film varies when measured over short timespans (minutes and hours) and long  
95 timespans (months), when scanned using different film scanners at different institutions, the consistency of  
96 dose response in the use of different batches of Gafchromic EBT3 film over several years, the energy  
97 dependence for different batch formulations, as well as the dependence of relative dose distribution  
98 measured on film depending on when film was scanned or the type of calibration that was applied. The

99 data presented in this work provides substantial improvement to the field of film dosimetry by addressing  
100 the limitations in the dosimetric recommendations presented in TG-235. In this work, we propose simplified  
101 novel methods of Gafchromic film dosimetry for point dose measurements and relative dose distribution  
102 measurements that allows for rapid film processing without compromising the accuracy of film dosimetry  
103

## 104 2. MATERIALS AND METHODS

### 105 2.1 Short-term evaluation

#### 106 2.1.1 Evaluation of dose response

107 Gafchromic EBT3 films (Ashland, Bridgewater, NJ, USA) were cut into  $3.8 \times 3.8 \text{ cm}^2$  squares, with each  
108 square labeled with the dose to be delivered: 0–40 Gy. Film squares were irradiated with a 16-MeV electron  
109 beam from a Varian Clinac 2100 (Varian, Palo Alto, CA, USA). The machine was calibrated to deliver 1  
110 cGy/MU at the depth of maximum dose ( $d_{\text{max}}$ ) in water for a  $10 \times 10 \text{ cm}^2$  field at a source-to-surface distance  
111 (SSD) of 100 cm, according to the TG-51 protocol.<sup>13</sup> Six films were designated for each dose group. After  
112 irradiation, a first set of three films per group were scanned at the following times: 5–30 minutes and 1–  
113 100 hours after irradiation. The second set of three films per group were scanned only once at 24 hours after  
114 irradiation. This analysis was done to examine if and how repeated scans obtained intermittently over a 24-  
115 hour period (additional illumination to film) would affect the measured optical density in the irradiated  
116 EBT3 film.

117 An Epson Expression 10000XL flatbed scanner (Seiko Epson Corporation, Nagano, Japan) was  
118 used to scan all films. Each scanned image was acquired in transmission mode, landscape orientation, 48-  
119 bit color, 72 dpi, and without color correction. The films were placed on the scanner at the same location  
120 with the aid of a cardboard cutout. The scanned film data were analyzed by measuring the netOD of the  
121 irradiated film square relative to an unirradiated (0 Gy) film square from the same batch. The red channel  
122 was used unless otherwise noted for single-channel dosimetry measurements. The mean pixel value of each  
123 scanned EBT3 film square was obtained from ImageJ from a  $2.5 \times 2.5 \text{ cm}^2$  square region of interest placed  
124 at the center of the film square. The mean pixel values measured for the three films in each dose group were  
125 averaged to acquire an averaged mean pixel reading. The netOD reading was determined by taking the  
126 base-10 logarithmic ratio of the averaged mean pixel reading from the unirradiated film squares,  
127  $Pixel_{\text{background}}$ , with the averaged mean pixel reading from the film squares irradiated to an absorbed  
128 dose,  $Pixel_{\text{dose}}$ , using the following equation:  $\text{netOD} = \log_{10}\left(\frac{Pixel_{\text{background}}}{Pixel_{\text{dose}}}\right)$ .

#### 129 2.1.2 Evaluation of relative dose distributions

130 The effects of time delay (irradiation end to film-scanning) on relative dose distributions from EBT3 films  
131 were evaluated on acquired PDD curves. Three film strips measuring  $4.5 \times 9.0 \text{ cm}^2$  were used. Each film

132 strip was placed inside an acrylic water tank that had a 2-degree tilt with the film oriented parallel to the  
133 beam and its edge at the water's surface by using a clamp to situate the film in place. The apparatus used is  
134 described by Arjomandy et al. for mounting films for a depth-dose irradiation in a water tank.<sup>14</sup> Each EBT3  
135 film strip was irradiated with a 16-MeV electron beam at 100 cm SSD and a field size of  $25 \times 25 \text{ cm}^2$  with  
136 a  $d_{\text{max}}$  dose of 20 Gy. After irradiation, the films were dried off with paper towels and scanned at timepoints  
137 ranging from 5 minutes to 100 hours post-irradiation using an Epson 10000XL flatbed scanner. For each  
138 image scanned, the netOD was obtained, which was then converted to dose using a script written in  
139 MATLAB based on a dose calibration curve. The calibration curve was generated from the netOD measured  
140 in the scanned film squares from the first set of films in the same batch (described in section 2.2.1) that  
141 were irradiated to 1–40 Gy at 5 minutes to 100 hours post-irradiation (5 min, 1 h, 24 h. and 100 h). The  
142 three PDDs were then averaged to produce a single PDD curve for each scanned timepoint investigated.

143 The time-delay and batch dependent changes on the relative dose distributions of the PDD curves  
144 was investigated. The films used for PDDs were scanned at the four timepoints noted above that had their  
145 respective timepoint-specific calibration applied (e.g. film scanned 1 hour post-irradiation had a calibration  
146 applied based on film scanned at 1 hour post-irradiation); in a separate analysis, the film PDDs were  
147 compared with each other by using a calibration obtained at a single timepoint (24 hours after irradiation).  
148 The calibrations used were from the calibration curve generated specific to the scanned image's respective  
149 timepoint (5 minutes to 100 hours), plus the calibration curve at 24 hours, for the film squares irradiated to  
150 1–40 Gy. To explore EBT3's batch-dependence, the films for 3 PDDs, scanned at the 24-hour timepoint,  
151 had calibrations applied from five separate EBT3 batches purchased within the same year (labeled Batch  
152 A-E). The calibration curve from each batch had been scanned at 24 hours after irradiation to doses of 0–  
153 50 Gy.

154

## 155 **2.2 Long-term evaluation**

### 156 *2.2.1 Evaluation of film response over several weeks*

157 EBT3 films irradiated for batch calibration purposes were scanned at 24 hours after irradiation and then  
158 rescanned at 2–39 weeks after irradiation to evaluate how the response of the irradiated EBT3 film changes  
159 over longer periods. The calibration films included EBT3 film squares irradiated to a dose of 0–50 Gy, with  
160 three films used for each dose point, and irradiated as described for the short-term evaluation (2.1.1). The  
161 netOD measured at 2–39 weeks was normalized to the netOD measured at 24 hours. This provided  
162 quantification of OD evolution with scanning delay.

163

### 164 *2.2.2 Film batch comparison over a 5-year period*

165 Calibration curves of EBT3 film from 14 different batches were acquired over a period of 5 years, from  
166 May 2016 to May 2021. The films had been irradiated to doses ranging from 0–50 Gy, with three films  
167 irradiated per dose. The films were scanned between 18 and 24 hours after irradiation and analyzed  
168 separately based on the red, green, and blue channels. To quantify the variation in netOD between different  
169 film batches over time, the coefficient of variation (COV), also known as relative standard deviation, in the  
170 netOD measured for each dose level was calculated by dividing the standard deviation of the netOD  
171 measured for each dose group from all 14 batches by the mean netOD value for each dose group measured  
172 from all 14 batches.

173

### 174 **2.3 Scanner dependence**

175 To determine the influence of choice of scanner on the netOD response, EBT3 film irradiated to an absorbed  
176 dose of 1, 4, 10, and 20 Gy was scanned with one Epson 10000XL, two Epson 11000XL (referred to as  
177 Epson 11000XL-1 and 11000XL-2), and one Epson V800 film scanner. The same films were scanned on  
178 the Epson 10000XL and the Epson 11000XL-1 at the same institution. The film scanned at collaborating  
179 institutions on the Epson 11000XL-2 and Epson V800 came from different EBT3 film batches that were  
180 irradiated at their respective institutions within the same year, with three films used per dose investigated.

181

### 182 **2.4 Energy dependence for different film batches**

183 To investigate the energy dependence of EBT3 film, films from four separate batches were irradiated with  
184 radiation sources of different energies. The dose range investigated was 0–12 Gy. The radiation sources  
185 were Cs-137 (0.662 MeV) and Co-60 (1.25 MeV) and the radiation beam energies produced from a clinical  
186 linear accelerator were 6 MV and 18 MV photons, and 20 MeV electrons.

187

## 188 **3. RESULTS**

### 189 **3.1 Short-term evaluation**

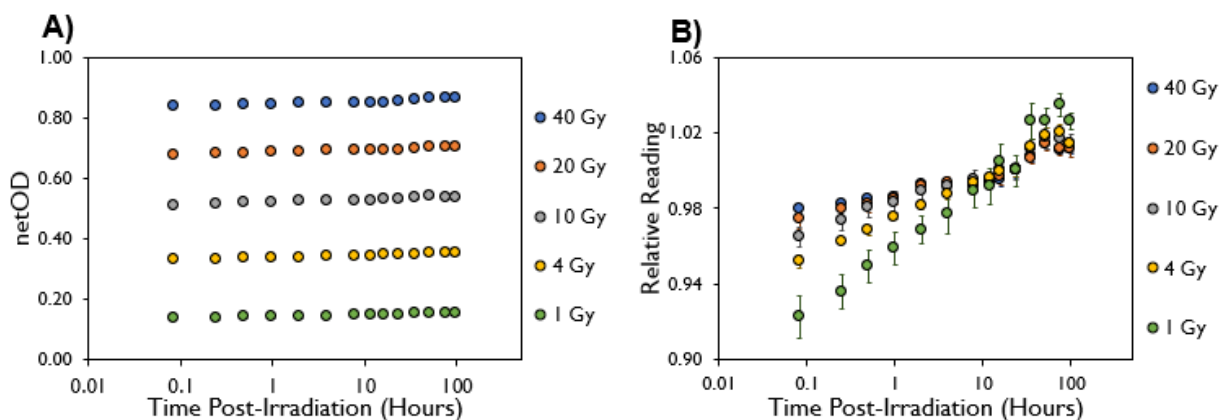
#### 190 *3.1.1 Evaluation of dose response*

191 The measured netOD in films that were scanned only once (at 24 hours after irradiation) were compared  
192 with the netOD measured in films that had been scanned ten times total at the 24-hour timepoint post-  
193 irradiation (Table S1). A negligible difference (<1%) was noted between the measured netOD (at the 24-  
194 hour timepoint) for film that had been scanned multiple times over a 24-hour period (measured at 0.08 h,  
195 0.25 h, 0.5 h, 1 h, 2 h, 4 h, 8 h, 12 h, 16 h, and 24 hours after irradiation) versus films that had been scanned  
196 only once, at 24 hours.

197

198

199 Figure 1A presents temporal evolution of netOD for films irradiated to absorbed doses 1–40 Gy.  
 200 Figure 1B presents the data of Figure 1A in terms of relative netOD (normalized to netOD for 24-hour  
 201 delay). The data in Figure 1B is also tabulated in Table S2. The rapid readout of film at 5 minutes after  
 202 irradiation to absorbed doses of 1–40 Gy led to measured netOD values that were 2%-8% lower than the  
 203 netOD value measured in film scanned at 24 hours after irradiation on the same scanner.  
 204



205  
 206 **Figure 1.** (A) Temporal dependence of EBT3 film response measured over a period of 100 hours and (B)  
 207 netOD normalized to 24 hours after irradiation. Error bars represent one standard deviation from three films  
 208 irradiated to each dose delivered.  
 209

### 210 3.1.2. Evaluation of relative dose distributions

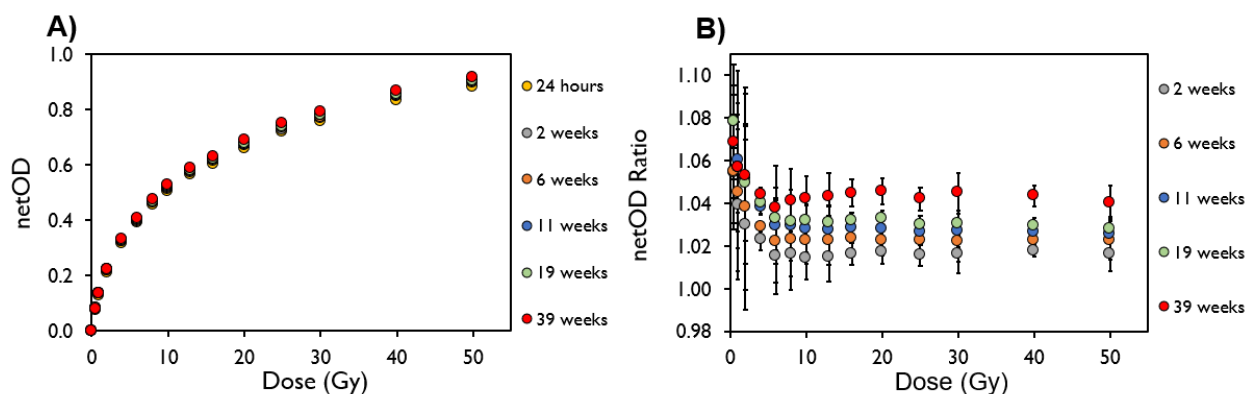
211 EBT3 film used to measure PDDs were scanned after delay of 5 minutes to 100 hours post-irradiation.  
 212 Measured netOD were converted to doses employing the delay-specific calibrations. This allowed for  
 213 determination of depth-doses, and consequently the depth-dose parameters of  $R_{30}$ ,  $R_{50}$ ,  $R_{80}$ , and  $R_{90}$ . These  
 214 values are presented in Table S3. For reference, the corresponding values from the commissioning of the  
 215 machine are shown. Table S3 also shows the relative percent difference in the measured beam parameter  
 216 values in films scanned at their respective timepoints with their respective time-specific calibration applied  
 217 versus what was measured when only the 24-hour calibration curve was applied. The depth-dose parameters  
 218 of  $R_{30}$ ,  $R_{50}$ ,  $R_{80}$ , and  $R_{90}$  measured in EBT3 film when only a general 24-hour calibration curve was applied  
 219 is listed in Table S4. The depths of the 16 MeV electron beam are within 1 mm of the values measured  
 220 from the TPS and within 1 mm of each other at the respective scanned timepoints (5 minutes to 100 hours  
 221 post-irradiation) regardless of which calibration curve was applied (Figure S1). Table S5 lists the beam  
 222 parameter values measured from the same EBT3 PDD films but with different batch calibrations applied  
 223 from calibration films scanned on the same scanner. That table also illustrates that the measured beam

224 parameters were within 1 mm of each other and within 1 mm of the beam parameter values measured by  
225 the TPS, despite the use of different batch calibrations.  
226

### 227 3.2 Long-term evaluation

#### 228 3.2.1 Evaluation of film response over several weeks

229 Figure 2 compares the netOD reading measured at 2–39 weeks after irradiation in comparison with  
230 measurements obtained at 24 hours after irradiation, taken from a single batch of film irradiated to 0.5–50  
231 Gy, with three films irradiated per dose investigated. Figure 2A shows calibration curves of films measured  
232 at their respective timepoints, and Figure 2B shows the relative difference between the measurement at 24  
233 hours and the measurements scanned at 2–39 weeks after irradiation. The relative difference in the measured  
234 netOD scanned several weeks after irradiation were largest in films irradiated to low doses (< 6 Gy). In  
235 quantifying the relative increase in netOD, the netOD measured at 2 weeks after irradiation was between  
236 1.6% and 5.5% higher over the investigated dose range. At the 6-week timepoint, the netOD in film  
237 continued to increase, with a percent increase in netOD (relative to the 24-h measurement) of 2.3% to 5.5%;  
238 at 11 weeks, the percent increase was 2.6% to 7.8%; at 19 weeks, the percent increase ranged from 2.8% to  
239 7.8%; at 39 weeks, the percent increase ranged from 3.8% to 6.8%. At doses greater than or equal to 6 Gy,  
240 the percent relative difference in netOD between the 24-h measurement and the 2-, 6-, 11-, 19- and 39-  
241 week timepoints stabilized and averaged at  $1.6 \pm 0.11\%$  (at 2 weeks),  $2.3 \pm 0.04\%$  (at 6 weeks),  $2.8 \pm 0.12\%$   
242 (at 11 weeks),  $3.1 \pm 0.15\%$  (at 19 weeks), and  $4.3 \pm 0.24\%$  (at 39 weeks).  
243

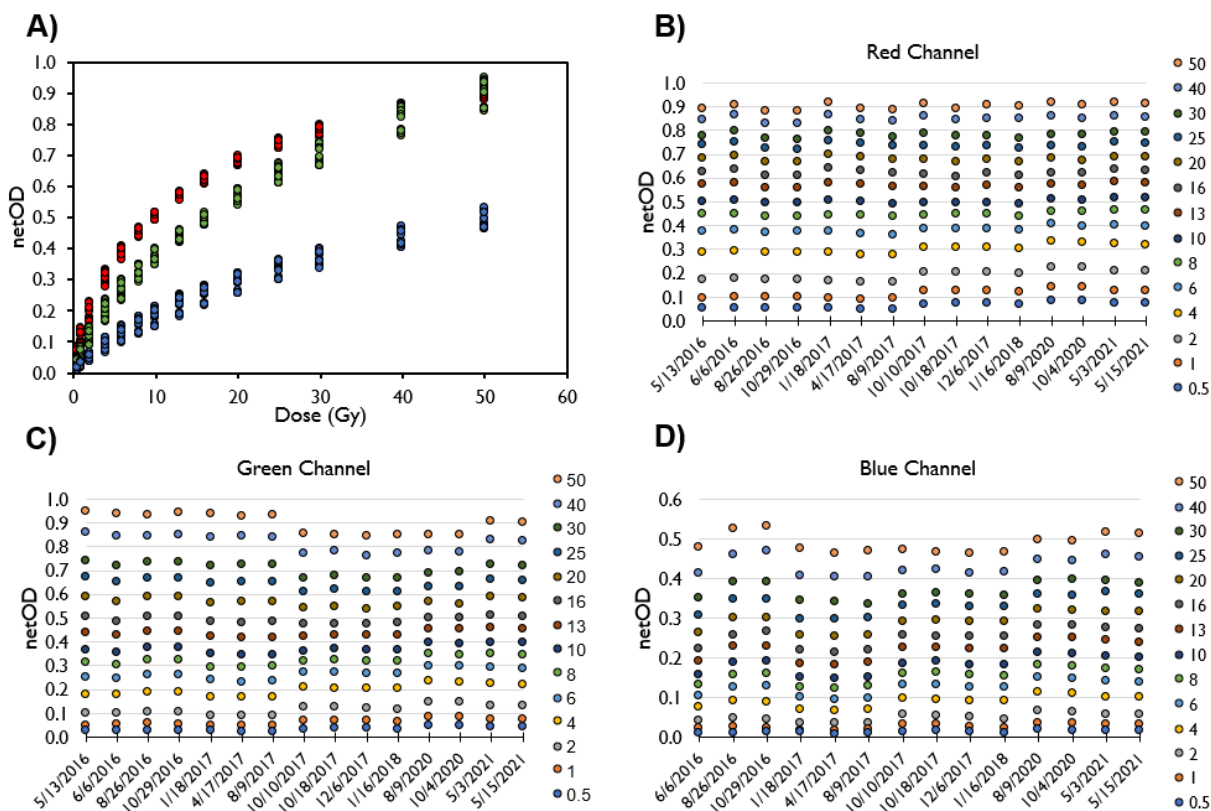


244  
245 **Figure 2.** (A) Dose response curve and (B) netOD ratio relative to the 24-h measurement of EBT3 film scanned  
246 at 24 hours, 2 weeks, 6 weeks, 11 weeks, 19 weeks, and 39 weeks after irradiation to doses of 0.5–50 Gy. Error  
247 bars represent one standard deviation from three measurements.  
248

#### 249 3.2.2 Film batch comparison over a 5-year period

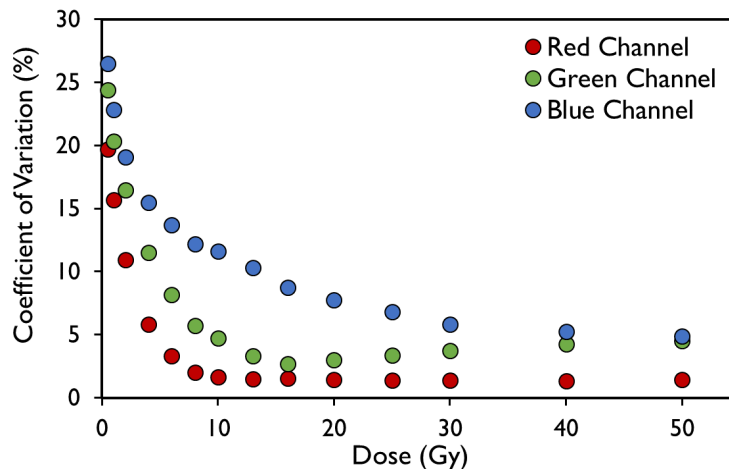


250 The dose response curves of EBT3 films scanned 18 to 24 hours after irradiation from 14 different batches  
 251 of EBT3 film collected from 2016 to 2021 with the red, green, and blue channel are shown in Figure 3. The  
 252 variation between different batch calibration curves from separate color channels was smallest for  
 253 measurements taken with the red channel and was largest in netOD measured in the blue channel. Figure  
 254 3B-D show the netOD specific to each dose value with the date that each batch of calibration curves were  
 255 scanned. No correlation was found between the variation in the measured signal for the different batches  
 256 investigated between the red, green, and blue channels.



257  
 258 **Figure 3.** (A) Dose response curve of EBT3 film data (16 MeV electrons, 14 calibration curves total)  
 259 scanned from 2016 to 2021 at 18 to 24 hours after irradiation to doses of 0.5–50 Gy with the red, green,  
 260 and blue channels. (B-D) The netOD measured at each dose point, with the indicated scan date, for the (B)  
 261 red, (C) green, and (D) blue channels.

262  
 263 The COV of the measured netOD values at each dose point evaluated for the red, green, and blue  
 264 color channels for all doses evaluated in 14 different batches of EBT3 film between 2016 and 2021 are  
 265 shown in Figure 4 and Table S6. The measured netOD for each dose value in the red channel showed the  
 266 smallest COV of all three color channels; a COV of 10% or less was observed in films irradiated to 6 Gy  
 267 or higher in the red and green channels, and in films irradiated to 16 Gy or higher in the blue channel.

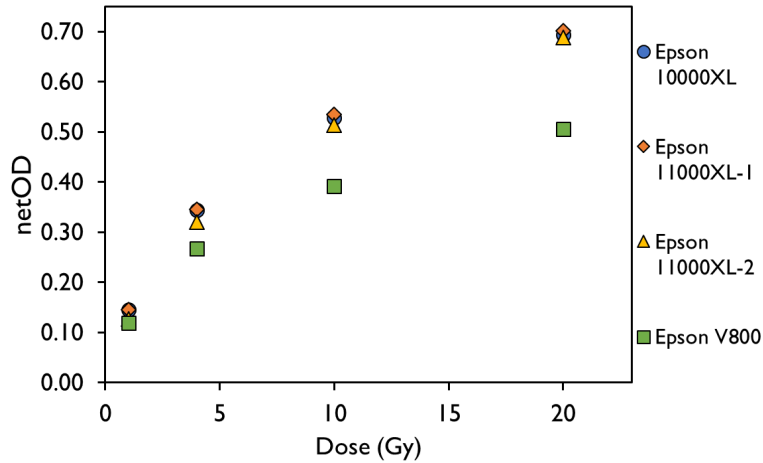


268  
 269 **Figure 4.** Coefficient of variation of EBT3 film data (14 calibration curves total) scanned at 18 to 24 hours  
 270 after irradiation from 2016 to 2021 with the red, green, and blue channels.

271  
 272 **3.3 Scanner dependence**

273 Figure 5 and Table S7 compare the netOD measured in the same films scanned at 24 hours after irradiation  
 274 with two different color scanners at the same institution (Epson 10000XL and Epson 11000 XL-1); also  
 275 shown are comparisons with measurements from different film batches irradiated to the same dose but  
 276 scanned at different institutions (Epson 11000XL-2 and Epson V800). The difference in the measured  
 277 netOD of the same film scanned on two separate scanners at the same institution was within 1% for the  
 278 Epson 10000XL and 11000XL-1, with the netOD measurement lower with the Epson 10000XL than with  
 279 the 11000XL-1 (difference of 0.1% to 1.1%). The netOD measured with two Epson 11000XL scanners at  
 280 two separate institutions were within 1.8% to 2.5% when using the same scanner type; the netOD measured  
 281 in film scanned with the Epson 11000XL-2 was consistently lower than the netOD measured in film  
 282 scanned with the Epson 11000XL-1. The netOD measured with the Epson V800 was substantially (2.6%  
 283 to 19.5%) lower than that in films scanned with the Epson 11000XL-1.

284

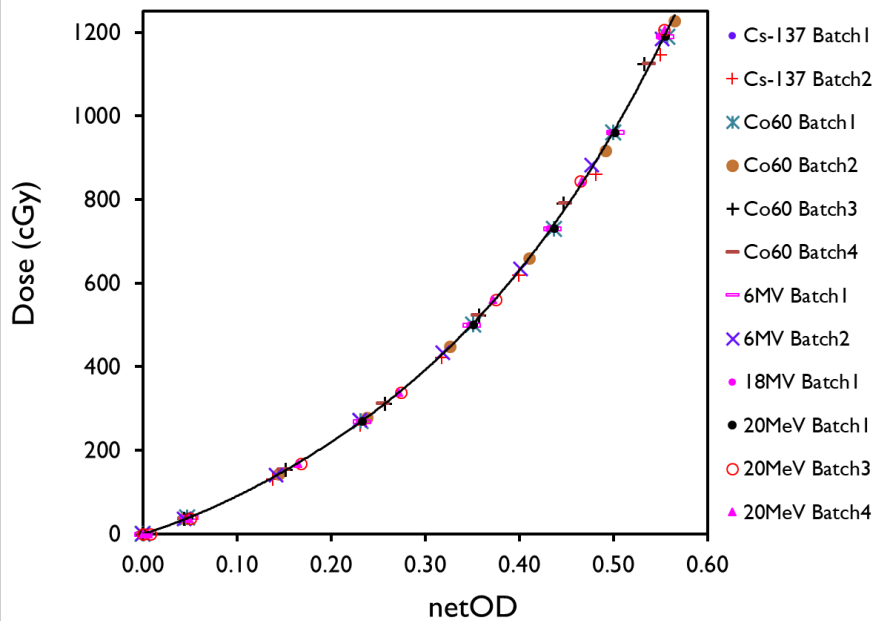


285  
 286 **Figure 5.** netOD values from EBT3 film scanned with Epson 10000XL, 11000XL, and V800 film scanners  
 287 at different institutions, measured at 24 hours after irradiation to 1, 4, 10, and 20 Gy. Error bars represent  
 288 one standard deviation from three films irradiated to each dose.

289  
 290

### 291 3.4 Energy dependence

292 Figure 6 shows the consolidated dose-response data points of EBT3 film from four different film batches  
 293 irradiated with different x-ray and electron beams at energies of 0.6–20 MeV, plotted with a polynomial  
 294 curve comprising of all the consolidated data (black line). The energy dependence and batch dependence  
 295 in EBT3 film irradiated in the mega-voltage energy range (including Cs-137 and Co-60) regardless of  
 296 modality type (photons/electrons) was found to be minimal with the relative percent difference between the  
 297 delivered dose with the dose measured from the polynomial fit being <12% for all of the batches and energy  
 298 combinations, with the highest relative difference observed in the datapoints acquired at 30-40 cGy dose  
 299 points. At delivered doses higher than 100 cGy, the relative percent difference between the delivered dose  
 300 and the dose measured from the polynomial fit was < 4% between the different batch and energy modality  
 301 types.



302  
 303 **Figure 6.** Dose response curve for EBT3 film from four different batches irradiated using Cs-137, Co-60,  
 304 and mega-voltage x-ray and electron beams at a dose range of 0-12 Gy.

305  
 306 **4 DISCUSSION**

307 **4.1 Short-term evaluation**

308 One key finding from this study was that repeat single scans of EBT3 film at different intervals within the  
 309 first 24-hours after irradiation did not have a significant effect on the resulting netOD, thereby confirming  
 310 the robustness and insensitivity of EBT3 film to the light produced from the Xenon cathode fluorescent  
 311 lamp in the Epson 10000XL scanner when scanned intermittently over a 24-hour period. Because each film  
 312 was scanned once at each timepoint considered (18 films), the lack of change in netOD indicates that the  
 313 number of scans obtained at each timepoint was not sufficient to affect the temperature of the scanner,  
 314 which can otherwise cause a change in the netOD reading.<sup>1,2,15</sup>

315 Increases in OD after irradiation limit the use of EBT3 film for film dosimetry, given that the user  
 316 must follow a timepoint-specific calibration procedure for accurate dosimetry. AAPM TG-235 recommends  
 317 a 16- to 24-hour wait time between irradiation and scanning to allow stabilization of any post-exposure  
 318 increase in signal, within the bounds of a clinic’s established protocol, or by adopting the one-scan protocol,  
 319 a simplified protocol that allows rapid film scanning and dose calculation by using a recalibration method  
 320 with patient film, reference film, and unexposed film as proposed by Lewis et al. in 2012.<sup>1,16</sup> Others have  
 321 reported using shorter wait times after irradiation to allow the OD in film to stabilize. Sharma et al 2021<sup>17</sup>  
 322 reported that the growth kinetics of EBT3 netOD stabilized as soon as 6 hours after irradiation of EBT3  
 323 film to doses of 1 Gy or higher, which is consistent with our findings. Borca et al. 2007<sup>3</sup> reported

324 stabilization in netOD growth as soon as 2 hours after irradiation for film irradiated to 1–4 Gy. Sharma et  
325 al. defined stabilization of the netOD as being within 2% of the netOD value at 24 hours, whereas Borca et  
326 al. defined it as being within 2.5% of the netOD value at 24 hours after irradiation. The results of these past  
327 studies and ours show that netOD in EBT3 film stabilizes earlier than the 16- to 24-hour interval  
328 recommended by TG-235 and that stabilization in film is strongly dependent on the dose delivered to the  
329 film of interest and the time the film was scanned post-irradiation. In the current study, we found that to be  
330 within 2% of its 24-hour netOD value, film irradiated to an absorbed dose of 4 Gy must be scanned at  
331 anywhere between 1 hour and 76 hours after irradiation, and for film irradiated to an absorbed dose of 1  
332 Gy, that interval was 4-24 hours after irradiation. Film irradiated to doses of 10 Gy or higher can be scanned  
333 within 30 minutes to 100 hours after irradiation and still be within 2% of its 24-hour netOD value.

334 For relative dosimetric measurements of dose distributions with EBT3 film, the use of (1) a time-  
335 specific calibration curve, (2) a standard 24-hour calibration curve from the same batch, or (3) a calibration  
336 curve from a different batch of film all showed insensitivity to the choice of calibration applied. Notably,  
337 this insensitivity was found for calibration curves generated from the same scanner that the measurement  
338 films were scanned on. Electron beam parameters at a depth beyond  $d_{\max}$  where the PDD curve is 30%,  
339 50%, 80%, and 90% of the maximum value measured in EBT3 film differed by no more than 1-2 mm  
340 relative to the PDD curves scanned at 24 hours after irradiation on the Epson 10000XL scanner, again  
341 demonstrating negligible effects from the use of time-specific and batch-specific calibration curves on  
342 relative dosimetry. Likewise, these beam parameter values deviated by  $\leq 1$  mm for the  $R_{50}$  value and  $\leq 1$ -2  
343 mm from the other electron beam parameter values reported by the TPS. However, use of calibration curves  
344 generated from different scanners would likely result in different PDDs, as we showed by the percent  
345 differences in netOD in Figure 5 and Table S7. From this we can conclude that the relative dose distribution  
346 is unperturbed based on when the user scans film as long as the dose calibration curve that was applied  
347 came from the same scanner that was used irrespective of film batch or the post-irradiation scan time of the  
348 measured film and calibration film.

349 Concerning the clinical use of film, with the development of patient specific QA equipment such  
350 as the ArcCheck (Sun Nuclear Corporation, Melbourne, FL, USA) and Delta4 (ScandiDos, Uppsala,  
351 Sweden), film is seldom used anymore in the evaluation of dose distributions of standard intensity-  
352 modulated radiation therapy plans<sup>18</sup>. However, their use in high-dose stereotactic treatments is still  
353 employed due to the unparallel spatial resolution that can be achieved with film. These treatments are most  
354 often delivered using high dose ( $> 8$  Gy) per fraction with emphasis on spatial performance and accuracy  
355 in the high-dose region of the dose distribution<sup>19</sup>. For a dose delivery of 8 Gy and utilizing a 24 hour  
356 calibration curve as the comparison, these films could be read out between 4 hours and 36 hours post  
357 irradiation with only an added uncertainty in dose determination of  $\leq 1\%$  (Figure 1 and Table S2). Higher

358 doses would expand this window further. Time specific calibration curves could also be employed which  
359 would then reduce this uncertainty further but with the increased effort of having to create specific  
360 calibration curves for multiple time points post irradiation. However, we show that the use of (1) a time-  
361 specific calibration curve, (2) a standard 24-hour calibration curve from the same batch, or (3) a calibration  
362 curve from a different batch of film all showed insensitivity to the choice of calibration applied in the  
363 relative dose distribution determination for doses above 6 Gy.

#### 364 **4.2 Long-term evaluation**

365 Our analysis of one batch of EBT3 film that was irradiated, scanned 24 hours later, and then rescanned 2–  
366 39 weeks after revealed that the EBT3 film continued to darken for several weeks after irradiation, with the  
367 netOD increasing by 1.5% to 7.8% relative to the original value scanned at 24 hours after irradiation at a  
368 dose range of 0.5–50 Gy. TG235 reported a 2.5% increase in the measured OD between 24 hours and 14  
369 days after irradiation, and another 2.5% increase 6 months later.<sup>1,20</sup> However, that report and the literature  
370 cited within it did not specify the dose range that yielded the 2.5%; our study showed that the increase in  
371 netOD several weeks after irradiation to be in fact dose-dependent with a greater percent increase in netOD  
372 measured in low doses (< 6 Gy) delivered to film. Palmer et al. found that darkening of EBT3 film after  
373 irradiation was a logarithmic function that continued to grow over their 3-month investigation period after  
374 doses ranging from 0 Gy to 14 Gy.<sup>21</sup> Their characterization of the absolute change in netOD over time  
375 showed that film irradiated to higher doses had a greater absolute change in netOD over time. Pocza et al.<sup>22</sup>  
376 evaluated darkening long-term of EBT2 film after irradiation to up to 2 Gy and found that OD increased by  
377 up to 15% for films scanned with the red channel at 18 months after irradiation relative to the original scan  
378 at 24 hours. Fuss et al.<sup>23</sup> reported that EBT film irradiated to 0.9–8.1 Gy and scanned 4 months later showed  
379 a 5.4%-12.4% increase in netOD relative to the netOD measured at 24 hours. From these data, we can  
380 conclude that beyond 24 hours, the extent of darkening in irradiated film is less severe than during the first  
381 few hours after irradiation. However, we found that the netOD continued to increase beyond 24 hours  
382 (Figure 1) and that this will continue for several months after irradiation (Figure 2). We further found that  
383 the relative increase in netOD was highest in films irradiated to lower doses, but the absolute increase in  
384 netOD was highest in films irradiated to higher doses. However, beyond 24 hours post irradiation, a constant  
385 relative increase in netOD as a function of time was found for doses of  $\geq 6$  Gy (Fig. 2B), thus allowing for  
386 the scanning and determination of the relative dose distribution at any time post 24h after irradiation without  
387 the use of correction factors for high dose plans.

388 In examining the calibration curves produced over the same dose range from multiple batches of  
389 EBT3 film over a period of 5 years, we found that the calibration was batch-dependent but overall had the  
390 least variation when the red channel and higher doses ( $\geq 10$  Gy) were used indicating that the red channel  
391 is the most suitable and most robust channel to use for applications related to single-channel dosimetry.

392 Some substantial variations in the green and blue channels seem to appear abruptly and remain consistent  
393 thereafter, as evidenced by the batches scanned in 10 October 2017 to 4 October 2020 with the green  
394 channel and batches scanned in 18 January 2017 to 16 January 2018 with the blue channel. The variation  
395 in calibration between batches depended on the color channel used, and no correlation was found between  
396 the variation in one channel and that of another between batches. Based on this data, one may argue against  
397 triple channel dosimetry for situations where the calibration curves are used across batches, given that  
398 introducing the green and blue channel introduces additional uncertainties as presented in this work. We  
399 acknowledge some limitations in the retrospective data such as uncertainties in the assumption that the  
400 doses delivered for all batches investigated were precisely matched; user-to-user scans of the film were  
401 negligible over that timeframe; and that the time of scanning after irradiation may not have been exactly as  
402 stated. However, the timeframe of scanning for these 14 batches (18 to 24 hours after irradiation) suggests  
403 that the relative change in netOD should be negligible (Table S2).

404 To the best of our knowledge, this is the first evaluation of multiple batches of EBT3 film irradiated  
405 to the same dose range over a period of several years with the goal of tracking variation in netOD across  
406 batches over a wide dose-range that is clinically relevant. However, batch homogeneity of EBT2 film was  
407 evaluated by Mizuno et al.,<sup>24</sup> who examined homogeneity in the netOD response on EBT2 film from five  
408 separate batches that had been irradiated at a single dose of 2 Gy. In comparing the netOD in EBT2 film  
409 irradiated with the same dose but from different batches, the differences in netOD were as high as 10% for  
410 the investigated dose. This finding is consistent with our observation of a COV of 10.9% in separate film  
411 batches analyzed with the red channel. Overall, the results of our study confirm the general recommendation  
412 regarding the use of calibration curves specific to each batch of film when EBT3 film is used for dose  
413 determination. However, because the shape of the calibration curve remains consistent for EBT3 film over  
414 a span of several years as shown in this study, the possibility of generating a “public” calibration curve that  
415 can be refitted based on fewer dose measurements specific to a film batch should be explored more closely  
416 as a way to simplify radiochromic film dosimetry.

417

### 418 **4.3 Scanner dependence**

419 The important take-away from these experiments is the need for consistency in the type of scanner used for  
420 irradiated EBT3 film. The same film irradiated on the Epson 10000XL and Epson 11000XL showed a  
421 difference in netOD values of up to 2% at the extremes of the dose range investigated, despite the  
422 similarities between the two scanners. These differences may have arisen from differences in optical  
423 scanning resolution or differences in how scanned images are processed from the internal components of  
424 the respective scanners. Regardless, these results highlight the need for consistency in the type of scanner  
425 used to acquire the scanned image from film for absolute dose conversions from film, because the error in

426 netOD between scanners will propagate and magnify in dose conversion in the application of calibration  
427 curves, thereby obfuscating the dose delivered to film. This experiment could have been improved by a  
428 cross-comparison of the same irradiated films, scanned at the same time after irradiation, on scanners of  
429 identical make and model (Epson 10000XL) and scanners of different design (such as the Epson V800) to  
430 compare variation between scanners of similar and different designs rather than relying on separate film  
431 measurements and scans obtained at different institutions.

432

#### 433 **4.4 Energy dependence**

434 Here, we have shown that the dose-response curves are minimally energy dependent at clinically relevant  
435 energy ranges from 0.662-20 MeV, confirming the observations from previous studies<sup>1,25,26</sup>, not only in the  
436 same batch of EBT3 film but also in different batches purchased in the same year. This demonstrates that  
437 film-calibration can be performed for any beam energy in the mega-voltage energy range provided that the  
438 film is also used for dosimetry in mega-voltage beams.

439

#### 440 **4.5 Recommendations**

441 Our findings on how time after irradiation, radiation dose, and type of scanner influence the results of using  
442 EBT3 film for dosimetry led us to propose the following general conclusions and guidelines (summarized  
443 in Table 1):

444         The dose response measured in EBT3 film between batches was found to have the smallest  
445 variation for red-channel analyses, and that higher doses showed less variation between batches, suggesting  
446 that use of the red channel for dose measurements is advantageous when dose is being measured from  
447 different batches of film. Furthermore, it is recommended that in calibrating film, the beam energy in the  
448 mega-voltage range for x-rays and electrons have no effect in the measured netOD even when measured  
449 between batches. We acknowledge that our findings on dose-response ranges are different from those of  
450 TG-235, which indicated that the useful clinical dose range for EBT3 film is 0.01–20 Gy<sup>1</sup>. However, in our  
451 study we have demonstrated the usability of EBT3 film beyond 20 Gy (up to 50 Gy) for single channel  
452 dosimetry, without indication of saturation, which is of considerable utility for novel treatment modalities  
453 such as FLASH radiotherapy where the usable dose range may extend beyond that recommended by the  
454 manufacturer, especially in treatments involving single fraction deliveries. We found that doses in excess  
455 of 10 Gy had substantially smaller uncertainty as to when the netOD was measured after irradiation relative  
456 to the measurement at 24 hours. Table 1 is listed below to provide a summary of observations made and  
457 their corresponding recommendations.

458

#### 459 **TABLE 1 Summarized Observations and Recommendations**



Observation	Recommendation
Number of intermittent scans (scanner illumination) has a negligible effect on netOD.	No correction factor needed for $\leq 10$ scans.
Scanner dependence is within 3% for scanners of similar make and model but is higher between scanners of different models.	Use the same scanner for calibration and dose readout.
No saturation in film response is observed within a dose range of 0-50 Gy.	Gafchromic EBT3 film is suitable for dosimetry measurements up to 50 Gy even for red channel.
NetOD measured with the red channel has lowest variation of the three channels between batches.	Use red channel to allow easier comparison of doses between batches.
No difference in shape of relative dose distribution regardless of whether time-specific or batch-specific calibration curves are used. This is only applicable if the same scanner was used for the measurement and calibration.	For relative dose measurements using higher doses, films can be scanned at any time without affecting accuracy, and the use of time-specific or batch-specific calibrations are not necessary.
Films with an absorbed dose of $>4$ Gy can be scanned between 1 hour and 100 hours after irradiation to be within a 2% uncertainty when analyzed with a standard 24h calibration curve. The corresponding numbers to be within 1% uncertainty would be between 4 hours and 36 hours post-irradiation.	If an extra uncertainty in dose readout is unacceptable in film measured outside its calibration time window, the tabulated correction factors can be applied.
Film scanned at a much longer timepoint post-irradiation (e.g. several weeks/months) were found to have a netOD approximately 2-8% larger than their 24-hour measurement at a dose range of 0.5-50 Gy.	Though not recommended, the netOD in film measured several weeks/months post-irradiation can be used to estimate the 24-hour post-irradiation netOD using correction factors presented in this study.
Calibration of EBT3 film with x-ray or electron beams in the mega-voltage energy range yields small difference in the netOD measurement even in different batches	The film response is independent of energy and modality (electrons/photons) in the mega-voltage range.

460

## 461 5 CONCLUSIONS

462 This analysis of the short-term, long-term, and inter-batch characteristics of EBT3 Gafchromic film  
463 irradiated to the full range of clinically relevant absorbed doses showed that the relative response in EBT3  
464 films scanned at different times can be used as a rule of thumb to estimate a correction factor for the netOD  
465 of EBT3 films measured at 24 hours after irradiation. We have shown that EBT3 film irradiated to low  
466 doses ( $<10$  Gy) required substantially longer post-irradiation wait times than films irradiated to higher doses  
467 ( $>10$  Gy) to be within 2% of the netOD value measured at 24 hours after irradiation. Likewise, when  
468 irradiated EBT3 film is stored in an environmentally stable location before its expiration, the netOD in the  
469 film continues to increase, with film irradiated to lower doses showing greater relative increases in netOD.  
470 However, we were able to characterize the dose dependent increase in the netOD over several months and

471 demonstrate a consistent percent increase in signal over-time for delivered doses at 6 Gy or higher, which  
472 may be useful for relative dose distribution measurements at this dose range and timeframe. The relative  
473 dose distribution of film in terms of normalized PDDs was shown to be robust when the same type of  
474 calibration specific to the default scanner was applied, regardless of which timepoint the calibration curve  
475 was specific for, or when the film was scanned, or which batch the calibration curve came from. Inter-batch  
476 differences in EBT3 film evaluated over a 5-year period revealed lower uncertainty in measured netOD  
477 values when film was irradiated to higher doses and analyzed with the red channel. In summary, we  
478 conclude that EBT3 film is a robust dosimeter for which the netOD value can be estimated when the time  
479 of scanning is known (relative to 24-hours after irradiation); that relative dose response curves remain  
480 largely unaffected when a scanner-specific calibration factor is applied; that EBT3 can be calibrated with  
481 any beam in the mega-voltage energy range; and that film response shows the least variance when the red  
482 channel is used for analysis and the films are irradiated to higher doses (up to 50 Gy).  
483

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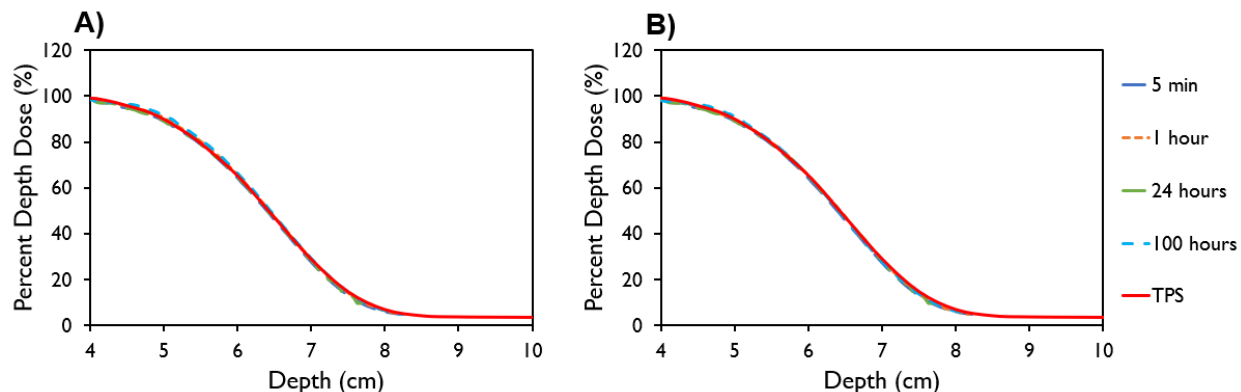
495

- 497 1. Niroomand-Rad A, Chiu-Tsao ST, Grams MP, et al. Report of AAPM Task Group 235  
498 Radiochromic Film Dosimetry: An Update to TG-55 [published online ahead of print  
499 2020/09/30]. *Med Phys.* 2020;47(12):5986-6025.
- 500 2. Marroquin EY, Herrera Gonzalez JA, Camacho Lopez MA, Barajas JE, Garcia-Garduno  
501 OA. Evaluation of the uncertainty in an EBT3 film dosimetry system utilizing net optical  
502 density [published online ahead of print 2016/09/30]. *J Appl Clin Med Phys.*  
503 2016;17(5):466-481.
- 504 3. Borca VC, Pasquino M, Russo G, et al. Dosimetric characterization and use of  
505 GAFCHROMIC EBT3 film for IMRT dose verification. *Journal of Applied Clinical Medical*  
506 *Physics.* 2013;14(2):158-171.
- 507 4. Liu K, Wang YF, Dona Lemus OM, Adamovics J, Wu CS. Temperature dependence and  
508 temporal stability of stacked radiochromic sheets for three-dimensional dose verification  
509 [published online ahead of print 2020/10/01]. *Med Phys.* 2020;47(11):5906-5918.
- 510 5. Wang YF, Dona O, Liu K, Adamovics J, Wu CS. Dosimetric characterization of a body-  
511 conforming radiochromic sheet [published online ahead of print 2020/02/27]. *J Appl Clin*  
512 *Med Phys.* 2020;21(3):167-177.
- 513 6. Devic S, Tomic N, Lewis D. Reference radiochromic film dosimetry: Review of technical  
514 aspects. *Physica Medica-European Journal of Medical Physics.* 2016;32(4):541-556.
- 515 7. Bazalova-Carter M, Liu M, Palma B, et al. Comparison of film measurements and Monte  
516 Carlo simulations of dose delivered with very high-energy electron beams in a polystyrene  
517 phantom. *Medical Physics.* 2015;42(4):1606-1613.
- 518 8. Karsch L, Beyreuther E, Burris-Mog T, et al. Dose rate dependence for different  
519 dosimeters and detectors: TLD, OSL, EBT films, and diamond detectors [published online  
520 ahead of print 2012/05/09]. *Med Phys.* 2012;39(5):2447-2455.
- 521 9. Romano F, Bailat C, Jorge PG, Lerch MLF, Darafsheh A. Ultra-high dose rate dosimetry:  
522 Challenges and opportunities for FLASH radiation therapy [published online ahead of print  
523 2022/04/12]. *Med Phys.* 2022;49(7):4912-4932.
- 524 10. Schuler E, Trovati S, King G, et al. Experimental Platform for Ultra-high Dose Rate FLASH  
525 Irradiation of Small Animals Using a Clinical Linear Accelerator. *International Journal of*  
526 *Radiation Oncology Biology Physics.* 2017;97(1):195-203.
- 527 11. Schuler E, Acharya M, Montay-Gruel P, Loo BW, Jr., Vozenin MC, Maxim PG. Ultra-high  
528 dose rate electron beams and the FLASH effect: From preclinical evidence to a new  
529 radiotherapy paradigm [published online ahead of print 2022/01/09]. *Med Phys.*  
530 2022;49(3):2082-2095.
- 531 12. Ashraf MR, Rahman M, Zhang RX, et al. Dosimetry for FLASH Radiotherapy: A Review  
532 of Tools and the Role of Radioluminescence and Cherenkov Emission. *Front Phys-*  
533 *Lausanne.* 2020;8.
- 534 13. Almond PR, Biggs PJ, Coursey BM, et al. AAPM's TG-51 protocol for clinical reference  
535 dosimetry of high-energy photon and electron beams. *Medical physics.* 1999;26(9):1847-  
536 1870.
- 537 14. Arjomandy B, Tailor R, Zhao L, Devic S. EBT2 film as a depth-dose measurement tool for  
538 radiotherapy beams over a wide range of energies and modalities [published online ahead  
539 of print 2012/02/11]. *Med Phys.* 2012;39(2):912-921.
- 540 15. Lewis D, Devic S. Correcting scan-to-scan response variability for a radiochromic film-  
541 based reference dosimetry system. *Medical Physics.* 2015;42(10):5692-5701.
- 542 16. Lewis D, Micke A, Yu X, Chan MF. An efficient protocol for radiochromic film dosimetry  
543 combining calibration and measurement in a single scan. *Medical Physics.*  
544 2012;39(10):6339-6350.

- 545 17. Sharma M, Singh R, Dutt S, Tomar P, Trivedi G, Robert N. Effect of absorbed dose on  
546 post-irradiation coloration and interpretation of polymerization reaction in the Gafchromic  
547 EBT3 film. *Radiat Phys Chem.* 2021;187.
- 548 18. Miften M, Olch A, Mihailidis D, et al. Tolerance limits and methodologies for IMRT  
549 measurement-based verification QA: Recommendations of AAPM Task Group No. 218  
550 [published online ahead of print 2018/02/15]. *Med Phys.* 2018;45(4):e53-e83.
- 551 19. Benedict SH, Yenice KM, Followill D, et al. Stereotactic body radiation therapy: the report  
552 of AAPM Task Group 101 [published online ahead of print 2010/10/01]. *Med Phys.*  
553 2010;37(8):4078-4101.
- 554 20. Andres C, del Castillo A, Tortosa R, Alonso D, Barquero R. A comprehensive study of the  
555 Gafchromic EBT2 radiochromic film. A comparison with EBT [published online ahead of  
556 print 2011/02/10]. *Med Phys.* 2010;37(12):6271-6278.
- 557 21. Palmer AL, Bradley D, Nisbet A. Evaluation and implementation of triple-channel  
558 radiochromic film dosimetry in brachytherapy [published online ahead of print 2014/09/11].  
559 *J Appl Clin Med Phys.* 2014;15(4):4854.
- 560 22. Pocza T, Zongor Z, Melles-Bencsik B, Tatai-Szabo DZ, Major T, Pesznyak C. Comparison  
561 of three film analysis softwares using EBT2 and EBT3 films in radiotherapy. *Radiol Oncol.*  
562 2020;54(4):505-512.
- 563 23. Fuss M, Sturtewagen E, De Wagter C, Georg D. Dosimetric characterization of  
564 GafChromic EBT film and its implication on film dosimetry quality assurance. *Phys Med*  
565 *Biol.* 2007;52(14):4211-4225.
- 566 24. Mizuno H, Takahashi Y, Tanaka A, et al. Homogeneity of GAFCHROMIC EBT2 film  
567 among different lot numbers. *Journal of Applied Clinical Medical Physics.* 2012;13(4):198-  
568 205.
- 569 25. Chiu-Tsao ST, Duckworth T, Zhang C, et al. Dose response characteristics of new models  
570 of GAFCHROMIC films: dependence on densitometer light source and radiation energy  
571 [published online ahead of print 2004/10/19]. *Med Phys.* 2004;31(9):2501-2508.
- 572 26. Bekerat H, Devic S, DeBlois F, et al. Improving the energy response of external beam  
573 therapy (EBT) GafChromic™ dosimetry films at low energies ( $\leq 100$  keV) [published  
574 online ahead of print 2014/02/11]. *Med Phys.* 2014;41(2):022101.

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577 **Supplementary Material**



578  
 579 **Figure S1.** The Percent Depth Dose (PDD) curve of a 16 MeV electron beam beyond the depth of  $d_{max}$   
 580 measured on EBT3 film with (A) time-specific calibration correction applied to film scanned at 5 min – 100  
 581 hours post-irradiation and (B) a general calibration correction (24-hour calibration) applied to film scanned  
 582 at 5 min – 100 hours post-irradiation.

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 585 **TABLE S1** Percent difference in net optimal density (netOD) from EBT3  
 586 films scanned once at 24 h after irradiation vs films scanned 10 times before  
 587 the 24-hours-after-irradiation time point. Films were irradiated to 1-40 Gy  
 588

Dose, Gy	Percent Difference in netOD, %
1	-0.40
4	0.85
10	0.19
20	-0.16
40	0.23

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 592 **TABLE S2** Measurements of netOD obtained at designated timepoints normalized  
 593 to the netOD measurement obtained at 24 hours

Time, h	Dose				
	40 Gy	20 Gy	10 Gy	4 Gy	1 Gy
0.08	0.98	0.97	0.96	0.95	0.92
0.25	0.98	0.98	0.97	0.96	0.94
0.5	0.98	0.98	0.98	0.97	0.95
1	0.99	0.99	0.98	0.98	0.96
2	0.99	0.99	0.99	0.98	0.97
4	0.99	0.99	0.99	0.99	0.98
8	0.99	0.99	1.00	0.99	0.99
12	0.99	0.99	1.00	1.00	0.99
16	0.99	1.00	1.00	1.00	1.00
24	1.00	1.00	1.00	1.00	1.00
36	1.01	1.01	1.01	1.01	1.03
52	1.01	1.01	1.02	1.02	1.03
76	1.01	1.01	1.02	1.02	1.03
100	1.01	1.01	1.01	1.01	1.03

594 **TABLE S3** Electron beam parameters for EBT3 films, scanned at various times after irradiation, with  
 595 timepoint-specific calibration curves applied, and parameters entered into the treatment planning system  
 596 (TPS) based on machine commissioning data. Also shown are the standard deviations of the parameters

597 from three irradiated films, and the percent difference relative to the measured values when a single  
 598 timepoint-specific (24-hour) calibration curve was applied  
 599

	<b>R<sub>30</sub>, cm</b>	<b>R<sub>50</sub>, cm</b>	<b>R<sub>80</sub>, cm</b>	<b>R<sub>90</sub>, cm</b>
<b>5 minutes</b>	6.93 ± 0.07 (0.4%)	6.38 ± 0.04 (0.6%)	5.47 ± 0.04 (0.7%)	4.96 ± 0.06 (0.2%)
<b>1 hour</b>	6.95 ± 0.06 (0.4%)	6.43 ± 0.06 (0.2%)	5.49 ± 0.03 (0.2%)	4.93 ± 0.05 (0.4%)
<b>24 hours</b>	6.96 ± 0.04	6.44 ± 0.02	5.47 ± 0.03	5.00 ± 0.06
<b>100 hours</b>	6.96 ± 0.07 (0.1%)	6.42 ± 0.07 (0.5%)	5.51 ± 0.06 (0.4%)	5.03 ± 0.02 (0.4%)
<b>TPS</b>	6.99	6.40	5.50	5.00

600 Rx, Depth in water of x% of the maximum dose value  
 601  
 602  
 603

604 **TABLE S4** Electron beam parameters for EBT3 films, scanned at various times after irradiation, with a  
 605 general 24-hour calibration curve applied, and parameters entered into the treatment planning system  
 606 (TPS) based on machine commissioning data. Also shown are the standard deviations of the parameters  
 607 from three irradiated films.  
 608

	<b>R<sub>30</sub>, cm</b>	<b>R<sub>50</sub>, cm</b>	<b>R<sub>80</sub>, cm</b>	<b>R<sub>90</sub>, cm</b>
<b>5 minutes</b>	6.96 ± 0.09	6.42 ± 0.05	5.51 ± 0.05	4.95 ± 0.07
<b>1 hour</b>	6.98 ± 0.04	6.44 ± 0.03	5.50 ± 0.04	4.95 ± 0.06
<b>24 hours</b>	6.96 ± 0.04	6.44 ± 0.02	5.47 ± 0.03	5.00 ± 0.06
<b>100 hours</b>	6.95 ± 0.06	6.45 ± 0.04	5.49 ± 0.04	5.01 ± 0.06
<b>TPS</b>	6.99	6.40	5.50	5.00

609 Rx, Depth in water of x% of the maximum dose value  
 610  
 611  
 612

613 **TABLE S5** Electron beam parameters for EBT3 films, scanned at the same time after irradiation, with  
 614 different batch calibration curves applied and parameters entered into the treatment planning system  
 615 (TPS) based on machine commissioning data. Also shown are the standard deviations of the parameters  
 616 from three irradiated films.  
 617

	<b>R<sub>30</sub>, cm</b>	<b>R<sub>50</sub>, cm</b>	<b>R<sub>80</sub>, cm</b>	<b>R<sub>90</sub>, cm</b>
<b>Batch A</b>	7.02 ± 0.01	6.43 ± 0.06	5.53 ± 0.03	4.98 ± 0.03
<b>Batch B</b>	6.97 ± 0.01	6.44 ± 0.06	5.53 ± 0.03	4.99 ± 0.06
<b>Batch C</b>	6.98 ± 0.05	6.45 ± 0.01	5.54 ± 0.03	4.99 ± 0.06
<b>Batch D</b>	6.94 ± 0.05	6.42 ± 0.02	5.44 ± 0.00	4.97 ± 0.07
<b>Batch E</b>	6.96 ± 0.04	6.42 ± 0.02	5.52 ± 0.01	4.97 ± 0.02
<b>24 hours</b>	6.96 ± 0.04	6.44 ± 0.02	5.47 ± 0.03	5.00 ± 0.06
<b>TPS</b>	6.99	6.40	5.50	5.00

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**TABLE S6** Coefficients of variation of EBT3 film data (14 calibration curves total) scanned at 18 to 24 hours after irradiation from 2016 to 2021 for the red, green, and blue channels

<b>Dose, Gy</b>	<b>Red, %</b>	<b>Green, %</b>	<b>Blue, %</b>
<b>0.5</b>	19.7	24.4	26.5
<b>1</b>	15.7	20.3	22.8
<b>2</b>	10.9	16.5	19.1
<b>4</b>	5.8	11.5	15.5
<b>6</b>	3.3	8.2	13.7
<b>8</b>	2.0	5.7	12.2
<b>10</b>	1.7	4.7	11.6
<b>13</b>	1.5	3.3	10.3
<b>16</b>	1.6	2.7	8.8
<b>20</b>	1.4	3.0	7.8
<b>25</b>	1.4	3.4	6.8
<b>30</b>	1.4	3.7	5.8
<b>40</b>	1.3	4.2	5.2
<b>50</b>	1.4	4.5	4.9

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**TABLE S7** Percent differences in netOD response between EBT3 film scanned on the Epson 11000XL-1 vs other film scanners at 24 hours after irradiation to 1, 4, 10, and 20 Gy

<b>Dose, Gy</b>	<b>Epson 10000XL, %</b>	<b>Epson V800, %</b>	<b>Epson 11000XL-2, %</b>
<b>1</b>	-0.13	-2.63	-1.87
<b>4</b>	-0.42	-7.73	-2.54
<b>10</b>	-1.21	-14.37	-2.11
<b>20</b>	-1.10	-19.55	-1.37

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