

# Transfer factor for carbon monoxide: a glance behind the scene

Jean-William Fitting

Service de pneumologie, Centre Hospitalier Universitaire Vaudois, Lausanne, Switzerland

## Summary

The transfer factor for carbon monoxide ( $T_LCO$ ) is widely used in pulmonary function laboratories because it represents a unique non-invasive window on pulmonary microcirculation. The  $T_LCO$  is the product of two primary measurements, the alveolar volume ( $V_A$ ) and the CO transfer coefficient (KCO). This test is most informative when  $V_A$  and KCO are examined, together with their product  $T_LCO$ . In a normal lung, a low  $V_A$  due to incomplete expansion is associated with an elevated KCO, resulting in a mildly reduced  $T_LCO$ . Thus, in case of low  $V_A$ , a seemingly “nor-

mal KCO” must be interpreted as an abnormal gas transfer. The most common clinical conditions associated with an abnormal  $T_LCO$  are characterised by a limited number of patterns for  $V_A$  and KCO: incomplete lung expansion, discrete loss of alveolar units, diffuse loss of alveolar units, emphysema, pulmonary vascular disorders, high pulmonary blood volume, alveolar haemorrhage.

*Key words: carbon monoxide transfer; pulmonary gas exchange; diffusing capacity*

## Introduction

The carbon monoxide transfer factor ( $T_LCO$ ) is widely used in lung function laboratories where it complements the measurement of lung volumes and of forced inspiratory and expiratory flows. The  $T_LCO$  is alternatively named the diffusing capacity ( $D_LCO$ ), but the former term is more appropriate for two reasons. First, this index is not uniquely determined by the diffusive characteristics of the lung, and second, it does not represent a maximal capacity in resting conditions because it easily increases with metabolic rate [1]. By measuring the surface area of the lung available for gas exchange, this test represents a unique window on the pulmonary microcirculation. Thus, the  $T_LCO$  is a key measurement in conditions like interstitial lung diseases and in the evaluation before surgery for lung cancer or for lung volume reduction in

emphysema. Furthermore, in the presence of normal lung volumes and spirometry, the  $T_LCO$  may be the sole abnormal test hinting to a pulmonary vascular disorder like chronic thromboembolic disease or other causes of pulmonary vascular obliteration.

Although the usefulness of the  $T_LCO$  is not disputed, the complexity of this test is not always fully appreciated. For instance, although introduced long ago by Marie Krogh in 1915 [2], this test was still fuelling a lively scientific controversy at the dawn of the XXI century! [3–5]. The aim of this article is first to recall some neglected principles of the  $T_LCO$ , and second to propose a practical scheme of interpretation which is largely inspired by the thorough work of Hughes and Pride [4, 6].

### Glossary:

CO:	carbon monoxide
$T_LCO$ :	carbon monoxide transfer factor (synonym: $D_LCO$ = carbon monoxide diffusing capacity)
$T_LCO_{SB}$ :	$T_LCO$ measured by the single-breath method
kCO:	rate constant for alveolar-capillary CO transfer (= permeability factor)
KCO:	carbon monoxide transfer coefficient
$V_A$ :	alveolar volume
TLC:	total lung capacity

$D_M$ :	membrane conductance
$\theta$ :	rate of reaction of CO with haemoglobin
QC:	pulmonary capillary blood volume
$P_B$ :	barometric pressure
$P_{H_2O}$ :	water vapour pressure
STPD:	standard temperature (0 °C) and pressure (760 mm Hg), dry
BTPS:	body temperature (37 °C) and pressure ( $P_B$ ) saturated with water vapour

## Measurement

The  $T_{LCO}$  measures the rate of transfer of CO from the alveoli to the blood. Inhaled carbon monoxide is used because of its very high affinity for haemoglobin: as a result, the plasma CO partial pressure remains close to zero, the gradient of partial pressure remains operational between the alveoli and the capillary blood, and the amount of CO transferred is limited by diffusion only. The single-breath  $T_{LCO}$  measurement ( $T_{LCO_{SB}}$ ) was introduced by Ogilvie et al. [7] and will be described here because it is the most widely used method.

The subject first fully exhales, then takes a rapid and full inspiratory vital capacity of a gas mixture composed of air, a tiny fraction of CO (0.003) and a fraction of an inert gas such as helium or methane. The breath is held for 10 seconds at complete inspiration before a rapid and full exhalation is made. After the first portion of exhaled gas has been discarded, gas is collected during mid-expiration as an alveolar sample for analysis of CO and of the inert gas. It is very important to control the quality of the manoeuvre by checking several points: that the inspiration is rapid enough (<2.5 s, or <4 s in case of airflow limitation), that the inspired volume is large enough (>90% vital capacity), and that the breath-holding time is correct ( $10 \pm 1$  s). From this, two primary measurements are made:

### Rate constant for alveolar-capillary CO transfer (= permeability factor, $k_{CO}$ ):

The initial alveolar fraction of CO is calculated as follows:

$$F_A CO_0 = F_I CO \cdot (F_A He / F_I He)$$

where:  $F_I CO$  = inspired fraction of CO  
 $F_A He$  = alveolar fraction of helium  
 $F_I He$  = inspired fraction of helium

During breath-holding, the alveolar fraction of CO decreases exponentially:

$$F_A CO_t = F_A CO_0 \cdot e^{-kt}$$

The permeability factor is calculated as follows:

$$k_{CO} = \frac{\log_e (F_A CO_0 / F_A CO_t)}{t}$$

where the unit for  $k_{CO}$  is:  $\text{min}^{-1}$

### Alveolar volume ( $V_A$ ):

$$V_A = V_I \cdot \frac{F_I He}{F_A He}$$

where:  $V_I$  = inspired volume  
the unit for  $V_A$  is: ml STPD

The  $T_{LCO}$  is then calculated as the product of the permeability factor and alveolar volume, divided by the effective barometric pressure:

$$T_{LCO} = \frac{k_{CO} \cdot V_A}{P_B - P_{H_2O}}$$

where:  $P_B$  = barometric pressure  
 $P_{H_2O}$  = water vapour pressure

The  $T_{LCO}$  is expressed in units of conductance:

$\text{mmol CO} \cdot \text{min}^{-1} \cdot \text{kPa}^{-1}$  (or  $\text{ml CO} \cdot \text{min}^{-1} \cdot \text{mm Hg}^{-1}$  in traditional units).

It is important to understand that the  $T_{LCO}$  is not the measurement of an actual physical variable. Rather, it is a calculation of what would be the flux of CO from the alveoli to the blood in the hypothetical condition of the subject's lungs being filled with 100% CO (which, if true, would expose to medico-legal consequences). Hence the introduction of alveolar volume which represents the volume of distribution of CO, and of barometric pressure which corresponds to the driving pressure for diffusion [6].

## Theoretical considerations

### Components of $T_{LCO}$

The  $T_{LCO}$  is made of two conductances in series: the *membrane conductance* ( $D_M$ ) which represents the diffusion component, and the *reactive conductance* ( $\theta \cdot Q_c$ ) where  $\theta$  is the rate of reaction of CO with haemoglobin and  $Q_c$  is the blood volume in the pulmonary capillaries. The  $D_M$  factor is reduced when the alveolar-capillary membrane surface is reduced or when its thickness is increased. The  $\theta$  factor varies with the concentration of haemoglobin: the low value of  $\theta$  explains the low values of  $T_{LCO}$  measured in anaemia [8].

### Confounding factors

Because of the effect of haemoglobin concentration [Hb],  $T_{LCO}$  has to be adjusted to the normal [Hb] in particular when anaemia is present or can be suspected. The adjusted value ( $T_{LCO}$  adj. or  $T_{LCO}$  corr.) is considered for assessing gas exchange.

Carboxyhaemoglobin (HbCO) reduces  $T_{LCO}$  by two mechanisms: first, it decreases the CO pressure gradient by increasing venous CO back pressure, and second, it decreases the mass of haemoglobin available for CO binding. The effect is a 1% fall of  $T_{LCO}$  for each 1% increment of [HbCO]. To avoid this problem it is recommended that the

subject refrains from smoking 24 hours before the test.

The  $T_{LCO}$  is influenced by altitude because oxygen and CO are in competition for Hb:  $\theta$  increases when alveolar  $PO_2$  falls. Thus,  $T_{LCO}$  increases by 0.31% per mm Hg decrease in inspired  $PO_2$ . This point has to be considered when the test is performed in a pulmonary function laboratory located at high altitude.

Exercise increases  $T_{LCO}$  by increasing pulmonary capillary blood volume ( $Q_c$ ). Thus,  $T_{LCO}$  increases by 20% for each increment of 5 L · min<sup>-1</sup> of cardiac output. It is recommended that the subject refrains from strenuous exercise and remains seated for at least 5 min before testing [9].

**The problem of  $V_A$  in airflow limitation**

Patients with chronic obstructive pulmonary disease (COPD), in particular those with emphysema, tend to have a higher than normal total lung capacity (TLC). Yet, the alveolar volume ( $V_A$ ) measured during the  $T_{LCO_{SB}}$  manoeuvre is low. This discrepancy between  $V_A$  and TLC is due to uneven ventilation distribution during the short breath-holding time leading to an incomplete mixing between the inspired gas and the residual volume gas. Indeed, the more severe is airflow limitation, the higher is the underestimation of TLC by  $V_A$ . As  $T_{LCO}$  is the product of  $kCO$  and  $V_A$  divided by effective barometric pressure, this results in an underestimation of the potential true  $T_{LCO}$  of the patient. However, the degree of underestimation is unknown, because poorly ventilated units are likely to be more severely affected by the disease. This is an inherent limitation of the  $T_{LCO_{SB}}$  in COPD. To circumvent this problem it has been proposed to use the  $V_A$  measured by plethysmography [1]. However, this would lead to an overestimation of true  $T_{LCO}$  because it would include poorly ventilated units and assign them a  $kCO$  equal to that of well ventilated units [4]. Moreover, this dual method is impractical and is consequently not applied.

**What is KCO (or  $T_{LCO}/V_A$ )?**

The carbon monoxide transfer coefficient (KCO) is often written as  $T_{LCO}$  divided by alveolar volume ( $T_{LCO}/V_A$ ). It is important to grasp what KCO actually represents. If we take the equation for  $T_{LCO}$ :

$$T_{LCO} = \frac{kCO \cdot V_A}{P_B - P_{H_2O}}$$

then, dividing by  $V_A$ :

$$KCO = T_{LCO}/V_A = \frac{kCO \cdot V_A}{(P_B - P_{H_2O}) \cdot V_A} = \frac{kCO}{P_B - P_{H_2O}}$$

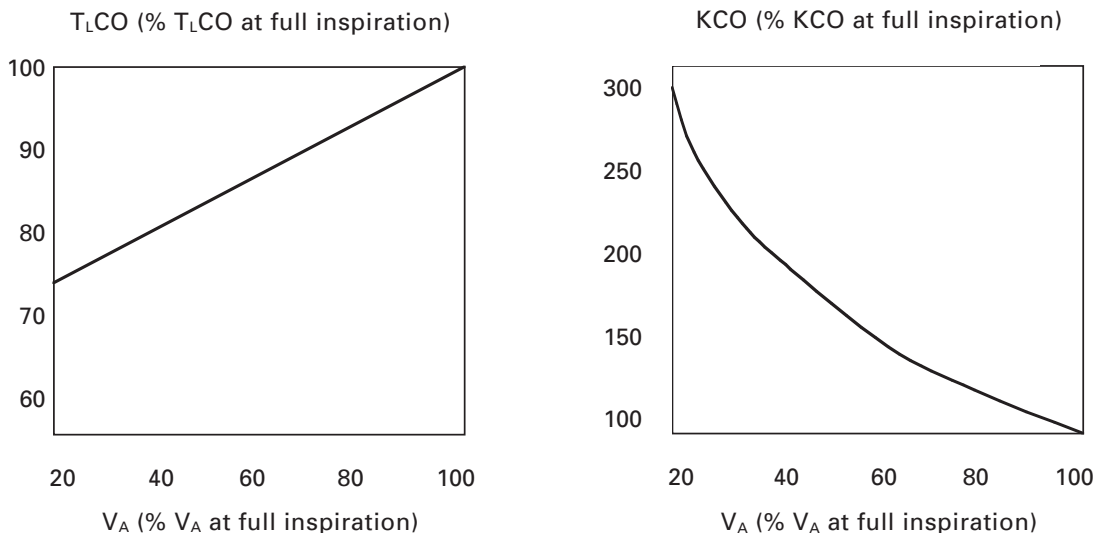
the units for KCO are: mmol CO · min<sup>-1</sup> · kPa<sup>-1</sup> · L<sup>-1</sup>, or ml CO · min<sup>-1</sup> · mm Hg<sup>-1</sup> · L<sup>-1</sup> in traditional units. In the latter case, note that  $V_A$  is expressed in ml STPD in the numerator because it represents a volume of CO, and in L BTPS in the denominator because it represents a volume of air.

Thus, the *transfer coefficient KCO* is simply another way to express the *permeability factor kCO*, one of the two primary measurements allowing to derive  $T_{LCO}$  [4, 6].

The expression  $T_{LCO}/V_A$  is misleading because it implies a “correction of  $T_{LCO}$  for alveolar volume”. According to this view, a low  $T_{LCO}$  with a low  $V_A$  and a normal KCO (or  $T_{LCO}/V_A$ ) would be interpreted as a lung of reduced volume but with normal transfer of CO. This is definitely wrong because in a normal lung, KCO increases exponentially when alveolar volume is reduced, as during a voluntary incomplete expansion, or during a reduced expansion in a patient with a neuromuscular disorder (Figure 1). This is due to an increase in the surface to volume ratio for diffusion per alveolus as the alveoli become smaller. Thus, when  $V_A$  is low, a seemingly “normal KCO” actually reflects an abnormal gas transfer.

**Figure 1**

Variation of carbon monoxide transfer coefficient (KCO) and transfer factor ( $T_{LCO}$ ) with lung expansion in normal subjects. The KCO,  $T_{LCO}$  and alveolar volume ( $V_A$ ) are expressed in percent of values measured at full inspiration. The KCO increases exponentially with decreasing  $V_A$ . As a result,  $T_{LCO}$  decreases only mildly with decreasing  $V_A$ .



### Practical considerations for interpretation of $T_LCO$

From the preceding considerations, it appears that the interpretation of  $T_LCO$  is unfortunately not straightforward. Nevertheless, this test is highly informative and useful if the following steps are taken [6]:

First, the quality of the manoeuvres must be scrupulously checked. This is now made easy by the display of error codes. A common failure is an insufficient inspired volume, whereas it should exceed 90% of vital capacity.

Second, KCO and  $V_A$  should be considered as the primary measurements and should be analysed along with  $T_LCO$ . The relationship between these variables can be seen as follows:

$$\begin{array}{rcccl} \text{KCO} & \cdot & V_A & = & T_LCO \\ \text{efficiency per} & & \text{number of} & & \text{gas exchange} \\ \text{lung unit} & & \text{contributing units} & & \text{capacity} \end{array}$$

For practical purposes, the most common disorders affecting  $T_LCO$  can be grouped in a limited number of pathophysiological or clinical entities.

#### 1) Incomplete lung expansion

The lung is normal but incompletely inflated, like in neuromuscular disorders, obesity, kyphoscoliosis, pleural effusion, or in case of a poorly performed test. The low  $V_A$  is associated with an elevated KCO. As a result,  $T_LCO$  is only mildly reduced, falling by 3% per 10% fall in  $V_A$ .

Case 1: 57-year-old man, acid maltase deficiency:

Vital capacity	50% pr.	$V_A$	64% pr.
Total lung capacity	65% pr.	KCO	141% pr.
FEV <sub>1</sub>	52% pr.	$T_LCO$	91% pr.
FEV <sub>1</sub> /FVC	100% pr.		

Case 2: 52-year-old woman, obesity (BMI = 64 kg · m<sup>-2</sup>):

Vital capacity	84% pr.	$V_A$	63% pr.
Total lung capacity	72% pr.	KCO	143% pr.
FEV <sub>1</sub>	61% pr.	$T_LCO$	91% pr.
FEV <sub>1</sub> /FVC	106% pr.		

#### 2) Discrete loss of alveolar units

There is a discrete loss of lung, for instance a whole lung, a lobe, or several units in several lobes, but the lung remaining is normal. Examples are pneumonectomy, lobectomy, lobar collapse, local destruction (post-TB, bronchiectasis), localized alveolar infiltrate (sarcoidosis). The loss of alveolar units is reflected by a low  $V_A$ . Because blood flow of lost units is diverted to remaining units, KCO increases slightly. As a result,  $T_LCO$  falls relatively less than  $V_A$ .

Case 3: 62-year-old man, post-pneumonectomy (right lung):

Vital capacity	43% pr.	$V_A$	45% pr.
Total lung capacity	55% pr.	KCO	110% pr.
FEV <sub>1</sub>	45% pr.	$T_LCO$	50% pr.
FEV <sub>1</sub> /FVC	104% pr.		

#### 3) Diffuse loss of alveolar units

The alveolar units most severely affected by the disease are lost, but the remaining lung is affected as well by the disease. Examples are diffuse fibrosis (idiopathic pulmonary fibrosis, connective tissue diseases, pneumoconiosis), alveolar infiltrates (inflammatory infiltrate, hypersensitivity pneumonitis, pneumocystis carinii pneumonia), cardiovascular disorders (pulmonary oedema, chronic heart failure). The  $V_A$  is low, KCO is low to "normal", and  $T_LCO$  is markedly reduced.

Case 4: 79-year-old man, pulmonary asbestosis:

Vital capacity	59% pr.	$V_A$	47% pr.
Total lung capacity	60% pr.	KCO	79% pr.
FEV <sub>1</sub>	65% pr.	$T_LCO$	37% pr.
FEV <sub>1</sub> /FVC	109% pr.		

Case 5: 75-year-old man, idiopathic pulmonary fibrosis:

Vital capacity	73% pr.	$V_A$	60% pr.
Total lung capacity	66% pr.	KCO	98% pr.
FEV <sub>1</sub>	77% pr.	$T_LCO$	59% pr.
FEV <sub>1</sub> /FVC	105% pr.		

Case 6: 73-year-old man, chronic heart failure:

Vital capacity	86% pr.	$V_A$	76% pr.
Total lung capacity	96% pr.	KCO	80% pr.
FEV <sub>1</sub>	81% pr.	$T_LCO$	61% pr.
FEV <sub>1</sub> /FVC	95% pr.		

Case 7: 45-year-old man, systemic lupus erythematosus with interstitial lung infiltrate and diaphragm weakness:

Vital capacity	46% pr.	$V_A$	45% pr.
Total lung capacity	63% pr.	KCO	104% pr.
FEV <sub>1</sub>	50% pr.	$T_LCO$	47% pr.
FEV <sub>1</sub> /FVC	109% pr.		

Comment: the interstitial lung disease and the diaphragm weakness both contribute to a low  $V_A$ . In case of diaphragm weakness with a normal lung, the KCO would be elevated, whereas the seemingly "normal" value observed here reflects the effect of interstitial disease.

#### 4) Obstructive lung disease

The  $V_A$  is low because of incomplete mixing between the inspired gas and the residual volume gas during the short breath-holding time. The KCO differs according to the underlying disease. In emphysema, KCO is low because of the loss of alveolar-capillary surface. As a result,  $T_LCO$  is se-

verely reduced. In contrast, KCO may be increased in asthma where the pulmonary microcirculation is preserved and cardiac output may be increased.

Case 8: 76-year-old man, pulmonary emphysema:

Vital capacity	68% pr.	V <sub>A</sub>	65% pr.
Total lung capacity	118% pr.	KCO	26% pr.
FEV <sub>1</sub>	30% pr.	T <sub>L</sub> CO	17% pr.
FEV <sub>1</sub> /FVC	44% pr.		

5) Pulmonary vascular disorders

Examples are pulmonary arterial hypertension, chronic thromboembolic pulmonary hypertension, vasculitis, sickle-cell disease, hepatopulmonary syndrome. The V<sub>A</sub> is normal or near normal, KCO is reduced due to the vascular disorder, and T<sub>L</sub>CO is reduced approximately to the same degree.

Case 9: 52-year-old woman, chronic thromboembolic pulmonary hypertension:

Vital capacity	123% pr.	V <sub>A</sub>	98% pr.
Total lung capacity	105% pr.	KCO	56% pr.
FEV <sub>1</sub>	101% pr.	T <sub>L</sub> CO	55% pr.
FEV <sub>1</sub> /FVC	88% pr.		

Case 10: 24-year-old woman, Takayasu's disease:

Vital capacity	88% pr.	V <sub>A</sub>	84% pr.
Total lung capacity	95% pr.	KCO	74% pr.
FEV <sub>1</sub>	79% pr.	T <sub>L</sub> CO	62% pr.
FEV <sub>1</sub> /FVC	95% pr.		

6) Increased pulmonary blood volume

Both KCO and T<sub>L</sub>CO are mildly to moderately increased when pulmonary capillary blood volume is increased, as in case of high cardiac output or of left-to-right shunt.

7) Alveolar haemorrhage

Intermittent alveolar haemorrhage occurs in anti-GBM disease, pulmonary vasculitis, systemic lupus erythematosus, and idiopathic haemosiderosis. The V<sub>A</sub> is mildly reduced by alveolar filling with blood, and KCO is markedly increased because inhaled CO reacts with extravascular haemoglobin. The KCO often increases to more than 150% of predicted, and a 30% increase in KCO over baseline values is suggestive of alveolar haemorrhage [10]. After haemorrhage ceases, the half-time of the return of KCO to baseline is 24 hours. It is essential to adjust KCO and T<sub>L</sub>CO to a normal haemoglobin concentration because of fluctuating anaemia in these patients [6].

Thus, by analysing V<sub>A</sub>, KCO and T<sub>L</sub>CO together one is able to discriminate between the most common abnormal patterns (Table 1). Although not straightforward, this analysis of T<sub>L</sub>CO is worth the effort because major therapeutic decisions may depend on this test, like performing surgery or initiating immunosuppressive or cytostatic therapy.

*Correspondence:*  
 Prof. J.W. Fitting  
 Service de pneumologie  
 CHUV  
 CH-1011 Lausanne  
 Switzerland  
 E-Mail: jfitting@chuv.hospvd.ch

**Table 1**  
 Common abnormal patterns of carbon monoxide transfer factor.

Condition	VA	KCO	TLCO
Incomplete lung expansion	↓↓↓	↑↑	↓
Discrete loss of alveolar units	↓↓↓	↑	↓↓
Diffuse loss of alveolar units	↓↓	↓	↓↓↓
Pulmonary emphysema	↓	↓↓	↓↓↓
Pulmonary vascular disorders	normal	↓↓	↓↓
High pulmonary blood volume	normal	↑	↑
Alveolar haemorrhage	↓	↑↑↑	↑↑

Single-breath method. VA: alveolar volume; KCO: carbon monoxide transfer coefficient; TLCO: carbon monoxide transfer factor.

## References

- 1 Cotes JE, Chinn DJ, Quanjer PH, Roca J, Yernault JC. Standardization of the measurement of transfer factor (diffusing capacity). Official statement of the European Respiratory Society. *Eur Respir J* 1993;6(Suppl. 16):41–52.
- 2 Krogh M. The diffusion of gases through the lungs of man. *J Physiol* 1915;49:271–96.
- 3 Chinn DJ, Cotes JE, Flowers R, Marks AM, Reed JW. Transfer factor (diffusing capacity) standardized for alveolar volume: validation, reference values and applications of a new linear model to replace KCO (TL/VA). *Eur Respir J* 1996;9:1269–77.
- 4 Hughes JMB, Pride NB. In defence of the carbon monoxide transfer coefficient KCO (TL/VA). *Eur Respir J* 2001;17:168–74.
- 5 Cotes JE. Carbon monoxide transfer coefficient KCO (TL/VA): a flawed index. *Eur Respir J* 2001;18:893–4.
- 6 Hughes JMB, Pride NB. *Lung Function Tests. Physiological principles and clinical applications.* W.B. Saunders, London, 2000.
- 7 Ogilvie CM, Forster RE, Blakemore WS, Morton JW. A standardized breath holding technique for the clinical measurement of the diffusing capacity of the lung for carbon monoxide. *J Clin Invest* 1957;36:1–17.
- 8 Roughton FJW, Forster RE. Relative importance of diffusion and chemical reaction rates in determining rate of exchange of gases in the human lung, with special reference to true diffusing capacity of pulmonary membrane and volume of blood in the lung capillaries. *J Appl Physiol* 1957;11:291–302.
- 9 American Thoracic Society. Single-breath carbon monoxide diffusing capacity (transfer factor). Recommendations for a standard technique-1995 update. *Am J Respir Crit Care Med* 1995;152:2185–98.
- 10 Ewan PW, Jones HA, Rhodes CG, Hughes JMB. Detection of intrapulmonary hemorrhage with carbon monoxide uptake. Application in Goodpasture's Syndrome. *N Engl J Med* 1976; 295:1391–6.

## The many reasons why you should choose SMW to publish your research

### What Swiss Medical Weekly has to offer:

- SMW's impact factor has been steadily rising, to the current 1.537
- Open access to the publication via the Internet, therefore wide audience and impact
- Rapid listing in Medline
- LinkOut-button from PubMed with link to the full text website <http://www.smw.ch> (direct link from each SMW record in PubMed)
- No-nonsense submission – you submit a single copy of your manuscript by e-mail attachment
- Peer review based on a broad spectrum of international academic referees
- Assistance of our professional statistician for every article with statistical analyses
- Fast peer review, by e-mail exchange with the referees
- Prompt decisions based on weekly conferences of the Editorial Board
- Prompt notification on the status of your manuscript by e-mail
- Professional English copy editing
- No page charges and attractive colour offprints at no extra cost

### Editorial Board

Prof. Jean-Michel Dayer, Geneva  
 Prof. Peter Gehr, Berne  
 Prof. André P. Perruchoud, Basel  
 Prof. Andreas Schaffner, Zurich  
 (Editor in chief)  
 Prof. Werner Straub, Berne  
 Prof. Ludwig von Segesser, Lausanne

### International Advisory Committee

Prof. K. E. Juhani Airaksinen, Turku, Finland  
 Prof. Anthony Bayes de Luna, Barcelona, Spain  
 Prof. Hubert E. Blum, Freiburg, Germany  
 Prof. Walter E. Haefeli, Heidelberg, Germany  
 Prof. Nino Kuenzli, Los Angeles, USA  
 Prof. René Lutter, Amsterdam, The Netherlands  
 Prof. Claude Martin, Marseille, France  
 Prof. Josef Patsch, Innsbruck, Austria  
 Prof. Luigi Tavazzi, Pavia, Italy

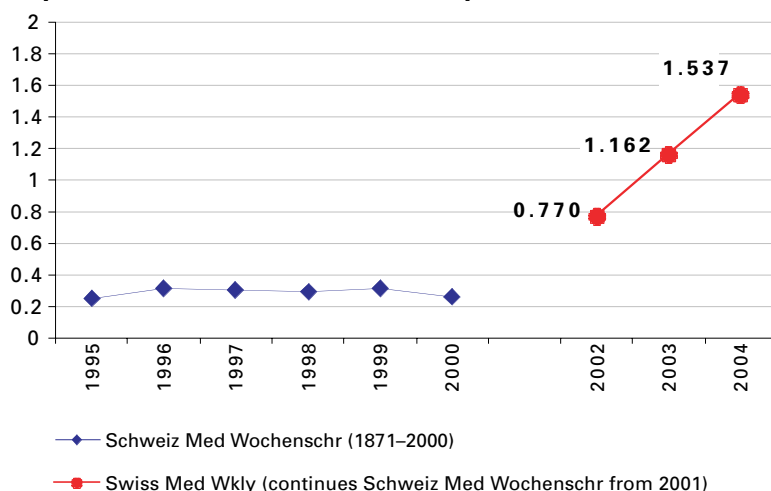
We evaluate manuscripts of broad clinical interest from all specialities, including experimental medicine and clinical investigation.

We look forward to receiving your paper!

Guidelines for authors:

[http://www.smw.ch/set\\_authors.html](http://www.smw.ch/set_authors.html)

### Impact factor Swiss Medical Weekly



All manuscripts should be sent in electronic form, to:

EMH Swiss Medical Publishers Ltd.  
 SMW Editorial Secretariat  
 Farnsburgerstrasse 8  
 CH-4132 Muttenz

Manuscripts: [submission@smw.ch](mailto:submission@smw.ch)  
 Letters to the editor: [letters@smw.ch](mailto:letters@smw.ch)  
 Editorial Board: [red@smw.ch](mailto:red@smw.ch)  
 Internet: <http://www.smw.ch>